

An Interactive Framework for Teaching Viscoelastic Modeling

Delf Kah^{1,*}, Ben Fabry¹, Richard C. Gerum¹

¹Biophysics Group, Department of Physics, Friedrich–Alexander University Erlangen–Nürnberg, Erlangen, Germany 91052

ABSTRACT Rheologic models consisting of combinations of linear elements, such as springs and dashpots, are widely used in biophysics to describe the mechanical and, in particular, the viscoelastic behavior of proteins, cells, tissue, and soft matter. Even simple arrangements with few elements often suffice to recapitulate the experimental data and to provide biophysical insights, making them an ideal subject for educational purposes. To provide students with an intuitive understanding of the mechanical behavior of spring and dashpot models, we describe a computer simulation tool, elastic viscous system simulator (ELViS), written in the JavaScript programming language for designing viscoelastic models via a graphical user interface and simulating the mechanical response to various inputs. As an example application, we designed a virtual laboratory course using ELViS that teaches the basic principles of viscoelastic modeling in a gamelike manner. We then surveyed 50 undergraduate students of a 1-semester course in biophysics who participated in the virtual laboratory course. Students felt that the course was a helpful addition to the lecture and that it improved learning success.

KEY WORDS viscoelastic model; e-learning; undergraduate

I. INTRODUCTION

Many biological systems show viscoelastic behavior: their responses to mechanical deformation show both elastic and viscous characteristics. When, in the first half of the 20th century, early biophysicists, such as Hill and Wyman, began to systematically characterize the viscoelastic mechanics of tissue, they sought to develop models that would be as simple as possible and yet could adequately describe the experimentally observed results. Today, the established framework to describe viscoelastic systems is a combination of linear springs (elastic elements) and linear dashpots (viscous elements). Figure 1 shows 3 of the most fundamental viscoelastic models that are routinely used to describe the mechanical behavior of cells (1) and tissue (2): the Maxwell model (Fig 1A); the Voigt model (sometimes also called the Voigt–Kelvin model; Fig 1B); and the Zener model (also found in the literature as standard linear solid or the Kelvin model; Fig 1C).

Even though these simple linear models cannot fully recapitulate the complexity of real biological structures, they were nonetheless fundamental to the development of mechanobiology and are still useful today. Hill famously investigated the mechanics of skeletal muscle and developed a simple viscoelastic model consisting of 3 elements, which could adequately describe the viscoelastic behavior he observed over decades of experimentation (3, 4). From the observation that an isolated frog skeletal muscle under isometric conditions instantly shortened as soon as the length constraints were

“*” corresponding author

Received: 30 September 2020

Accepted: 8 February 2021

Published: 25 June 2021

© 2021 Biophysical Society.

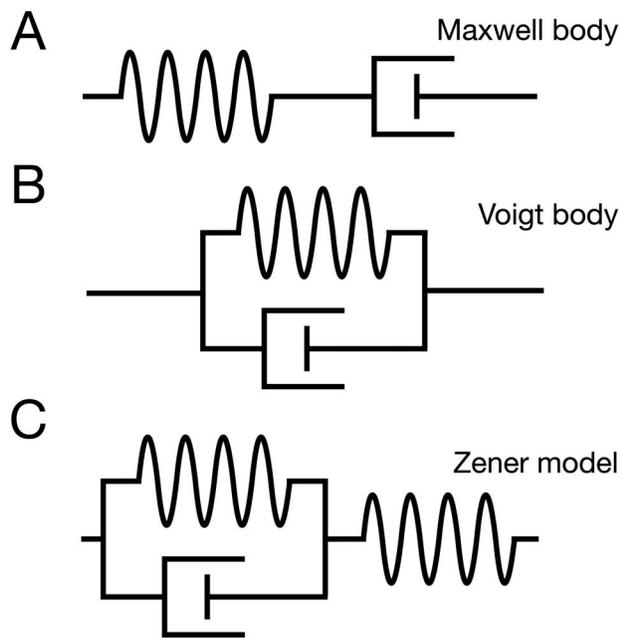


Fig 1. Basic viscoelastic model systems: (A) Maxwell; (B) Voigt; and (C) Zener.

removed (“quick-release experiment”), Hill deduced that a mechanical muscle model must include an elastic element in a series (5). From investigating the force and velocity relation of active muscles, he concluded that there must also be a damping element in series to the elastic element (6, 7).

In more recent studies, simple viscoelastic models are often used as a basis for a more complex modeling of biological matter. Applications range from the molecular to the macroscopic level, e.g., for the characterization of the mechanics and acting forces at focal adhesions (8), cells (9), intermediate filaments (10), ankle ligaments (11), and lung tissue (12).

The cytoskeleton is a good example to illustrate the implications of viscoelasticity on the function of different levels of structural hierarchy. On a molecular level, stiffness and force generation in muscle cells (and to a considerable degree also in nonmuscle cells) is attributable to actomyosin bridge formation (13). The elastic properties of the actomyosin bridges, in turn, are attributable mostly to the enthalpic elasticity of the S2-domain, the hinge region between the myosin head and tail (14). Upon bond breakage, any elastic energy is

dissipated, giving rise to frictional properties (15).

Cross-linking molecules other than myosin allow actin and other cytoskeletal filaments (microtubules, intermediate filaments) to form networks, which by similar enthalpic and bond breakage mechanisms, as in actomyosin bridges, exhibit elastic and dissipative properties (16). Moreover, cytoskeletal filaments exhibit thermal fluctuations, giving rise to entropic elastic properties (17), and because these fluctuations occur in the aqueous environment of the cytosol, viscous friction follows (18).

The simultaneous existence of both elastic and dissipative properties is a universal property of all solid matter, biological and nonbiological, as noted by Kohlrausch (19) when he observed the creep behavior of silk threads, metal wires, and glass fibers. The investigation of the viscoelastic properties of biological matter in particular has led to scientific findings that go beyond the mere characterization of material properties. For example, it has long been established that blood, due to cellular components, has not only viscous but also elastic properties (20). The viscoelastic properties of blood samples can be used to estimate the mechanics of erythrocytes (21), alterations of which may be indicative of certain diseases, such as malaria (22).

As an example, at a higher structural level, artery walls are routinely represented as spring and dashpot models to account for viscoelastic properties (e.g., hysteretic properties in the stress–strain relationship during wall expansion and contraction due to blood pressure changes) (23). Viscoelastic modeling is an important tool for understanding arterial diseases and for developing treatment options (24).

With only a few simple elements, viscoelastic models can describe the mechanical responses of a wide range of biological matter. They are, therefore, part of the basic syllabus of lectures on biomechanics, regardless of the field of study. For example, the Hill muscle model can be taught from a purely physiological point of view in a medical lecture class, it can be used as a starting point for teaching the molecular biophysics of motor proteins, or it can serve as

an example in a teaching unit for students with an engineering background in which students code their own computer simulations (25). As another example, a hands-on practical class has recently been described in which students build a low-cost tensile testing system, investigate the load and deformation behavior of different materials, and describe it with the Kelvin model (26). Teachers can find a good introduction into the concepts of viscoelastic modeling in the textbook by Howard (27). For courses particularly on biophysics, it is worth looking at the textbooks by Fung (2), Jacobs et al. (28), and McMahon (14), the latter of which offers a detailed description about Hill's findings on muscle mechanics.

Although the mechanical behavior of a single spring and a single dashpot is simple, the behavior of linear combinations of these 2 elements can quickly become surprisingly complicated. To give students a more intuitive understanding of this fundamental concept of biomechanics, we developed an elastic viscous system simulator (EIViS) that is intended as an interactive hands-on tool for teaching and understanding viscoelastic systems. With EIViS, students can build viscoelastic systems consisting of springs, dashpots, and internal force generators and investigate responses to external forces and deformations in a virtual lab. The software is written in the JavaScript programming language so that the lecturer can host it on a server for students to access it via a standard web browser, without the need to install additional software.

We provide the source code for EIViS in an online repository (<https://github.com/rgerum/EIViS>) under an open MIT license. The software framework can be used to program custom teaching modules involving viscoelastic systems. To demonstrate this, we developed a gamelike online lesson unit using EIViS, in which the user plays through 13 levels, starting with the basics of springs and dashpots and ending with the Hill muscle model. This lesson can be used out of the box as an introduction to viscoelastic systems without requiring students or lecturers to have programming skills. It is best suited for undergraduate courses in

biophysics or biomechanics, under supervision in a classroom setting, or as an online homework assignment. We let students of an undergraduate course on biomechanics (aimed at bachelor's and master's students) test the EIViS lesson as an online homework unit, and the subsequent evaluation indicates that the students gained a better understanding of the principles of viscoelastic modeling.

The electronic-learning (e-learning) lesson presented here is intended as a teaching unit to introduce the basic principles of viscoelastic modeling and to give students an intuitive understanding of creep and stress relaxation responses. In a subsequent lesson within a curriculum on viscoelastic systems, students will typically derive the differential equations that describe linear spring–dashpot networks. They will then go on to solve them for simple cases (e.g., the response to a force step) in the time domain and can use EIViS to verify that the results are correct. Next, and beyond what the interactive framework presented here covers, a typical curriculum might introduce the Laplace transform to more efficiently compute the steady-state response of viscoelastic systems to oscillatory forces and deformations.

II. SCIENTIFIC AND PEDAGOGIC BACKGROUND

The standard way of teaching viscoelastic modeling is to first introduce the 2 main building blocks: springs and dashpots. Springs (Hookean elements) display elastic properties and obey Hooke's law

$$F_{\text{spring}} = k \cdot \delta \quad (1)$$

where F_{spring} is the force acting on the spring, k is the spring constant, and δ is the deformation of the spring. Dashpots (Newtonian, viscous, or frictional elements) are used to model the viscous or more generally the dissipative properties of fluids. The force F_{dashpot} that is needed to deform a dashpot with a constant velocity v is given by the equation of motion for Newtonian fluids

$$F_{\text{dashpot}} = \gamma \cdot v \quad (2)$$

whereby γ is the damping (or drag) coefficient. The mass of the system can be neglected for overdamped motion, which is typically assumed for models of biological matter. For instance, for a Voigt body (see Fig 1B) that is connected to a mass m in a series, the overdamped approximation is valid for $\gamma^2 \gg 4mk$ (27). It is instructive for students to verify the overdamped approximation, for instance, for a protein in water with a mass in the order of 100 kDa and a stiffness on the order of 1 pN/nm.

To model biological matter with both viscous and elastic properties, one can connect the spring and dashpot elements with each other. The connection points (nodes) can either be movable or fixed. Movable nodes imply that the deformations of elements connected to that node have the same total value. Fixed nodes are used to connect elements to a static rigid structure with infinite stiffness (e.g., a wall).

Analogous to electrical circuits, linear elements can be connected in series or in parallel. For instance, the Voigt body (dashpot and spring in parallel) represents a compliant object that is deformed in a viscous fluid. To calculate the total force or displacement of a viscoelastic system, students must first understand some basic rules of how forces and deformations are distributed between serial and parallel elements. In the following, we consider only connections of linear elements via movable nodes. As a direct consequence of Newton's third law, the forces F_1 and F_2 acting on 2 (massless) linear elements connected in series are the same and have the same absolute value as the total force of the arrangement F_{series} . The total force of 2 linear elements connected in parallel F_{parallel} is the sum of the individual forces.

$$F_{\text{series}} = F_1 = F_2 \quad (3a)$$

$$F_{\text{parallel}} = F_1 + F_2 \quad (3b)$$

It can be intuitively understood that the total deformation of 2 elements in a series δ_{series} must be the sum of the individual deformations δ_1 and δ_2 , whereas the total deformation of 2 elements in a parallel arrangement δ_{parallel} must

be equal to the individual deformations.

$$\delta_{\text{series}} = \delta_1 + \delta_2 \quad (3c)$$

$$\delta_{\text{parallel}} = \delta_1 = \delta_2 \quad (3d)$$

Using Eqs. 3a–3d, as well as Hooke's law (Eq. 1), students should be able to deduce that the total spring constant of a parallel arrangement of 2 springs k_{parallel} must be the sum of the individual spring constants k_1 and k_2 . For series arrangements, the total compliance ($1/k_{\text{series}}$) is the sum of the individual compliances.

$$k_{\text{parallel}} = k_1 + k_2 \quad (4a)$$

$$1/k_{\text{series}} = 1/k_1 + 1/k_2 \quad (4b)$$

The total damping coefficient of 2 dashpots in serial and parallel arrangements behave analogous to Eqs. 4a and 4b. Also, Eqs. 3a–3d and Eqs. 4a and 4b can be expanded for an infinite number of serial or parallel elements.

The mechanical behavior of the viscoelastic model is described by the response function, which links the input to the system (e.g., a change in force) with its output (e.g., total deformation). To find the response function, one needs to use Eqs. 3a–3d and Eqs. 4a and 4b to derive a differential equation that describes the whole system. For complex interconnected viscoelastic models with many linear elements, it is useful to divide the arrangement into subsystems, derive the total forces, and spring constants of these subsystems and recombine them into expressions for the entire model. However, even if the response function is found, it might be difficult to solve the differential equation for a given force or deformation input by using pen and paper. One common trick is to transform the response function (and the input function) into the Laplace domain (29). For typical forms of force or deformation inputs, such as the Heaviside step function or the Dirac delta function, the Laplace representations can be found in lookup tables (30), and it can be easier to derive the response of the viscoelastic answer in the Laplace domain and then retransform it into the time domain than it would be to solve the differential equation in the time domain.

Although manually solving the response of viscoelastic systems can be a good exercise for students (e.g., with a background in physics or engineering), it is also an ideal opportunity for teaching computer-based numeric approaches (25). Even if the focus and schedule of the teaching unit does not allow for longer programming tasks for the students, numeric computer simulation programs can be useful to strengthen the student's intuitive understanding of viscoelastic systems. Therefore, a simulation program is desirable in which students can design viscoelastic model systems and test the response to different inputs. We present such a program with the ELViS in this article.

III. MATERIALS AND METHODS

A. Software description

ELViS uses a JavaScript framework (on the basis of the D3.js library) (31) for creating viscoelastic systems and for numerically solving the response to input forces and displacements and for visualization. Supplemental Material S1 describes the mathematical details for calculating the mechanical reaction of viscoelastic systems.

In brief, a system consisting of N nodes that connect massless linear elements is represented by a system of linear equations. Each node is characterized at every discrete time point t by a displacement δ_i^t and a force F_i^t . Its velocity v is defined indirectly as

$$v_i^t = (x_i^t - x_i^{t-1})/\Delta t \quad (5)$$

This indirect coding of speed has the advantage that the mechanics of the viscoelastic system can be described with less equations compared with having separate equations for x and v . Also, problems with infinite speeds, which can result from jumps in the system input, are eliminated (this is, for example, a problem with the sudden deflection of a single spring). As described in section II, nodes can either be fixed or free. For fixed nodes, the displacement is provided as a boundary condition, and the force F_i^t is an unknown variable. For free nodes, the force is provided as a boundary condition, and the displacement δ_i^t is

an unknown variable. The system of linear equations is then solved analytically for these unknown variables by using a matrix inversion. For each time step t , this analytic solution is used to calculate the forces F_i^t of the fixed nodes and the displacements δ_i^t of free nodes.

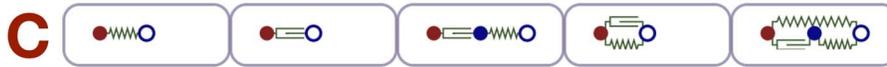
The source code is available as open-source software under the MIT license at GitHub. We give 2 example programs that can be realized with the ELViS framework: an open mode, where students can freely create viscoelastic systems in a drag and drop editor and simulate the answers to different inputs and an interactive lesson in 13 levels that teaches the basic concepts described in section II and ends with a final level about the Hill muscle model. Both the open mode (<https://rgerum.github.io/ELViS/>) and the lesson (<https://rgerum.github.io/ELViS/question.html>) can be tried on GitHub.

In the open mode, all features of ELViS are demonstrated. Supplemental Video S1 gives a short overview of the features of the open mode. The graphical user interface is shown in Figure 2. In the drag and drop editor (Fig 2A), the user can create a new spring by clicking at a node, keeping the mouse clicked, moving the cursor somewhere else, and releasing the mouse when a new node appears. Parallel arrangements are created by releasing the mouse at another existing node. When users create a new spring, they can click on it and change its properties in the element properties menu (Fig 2B), where it can be changed into a dashpot or an internal force generator. It is also possible to change the spring constant, damping coefficient, or amplitude force, respectively. This way, one can create complex arrangements of linear elements in series or in parallel.

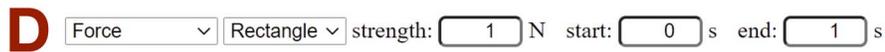
As an alternative approach to design a custom model system, the user can select and combine 5 preconfigured basic viscoelastic systems from the example menu (Fig 2C): a single spring; a single dashpot; a Maxwell body; a Voigt body; and a Kelvin body. In the input menu, (Fig 2D), the user can change between an input force and displacement and can change the shape of the input (rectangle, delta peak, theta function, or ramp), as well as its amplitude and time course. By selecting a ramp

ELViS-Simulator

Examples



Input

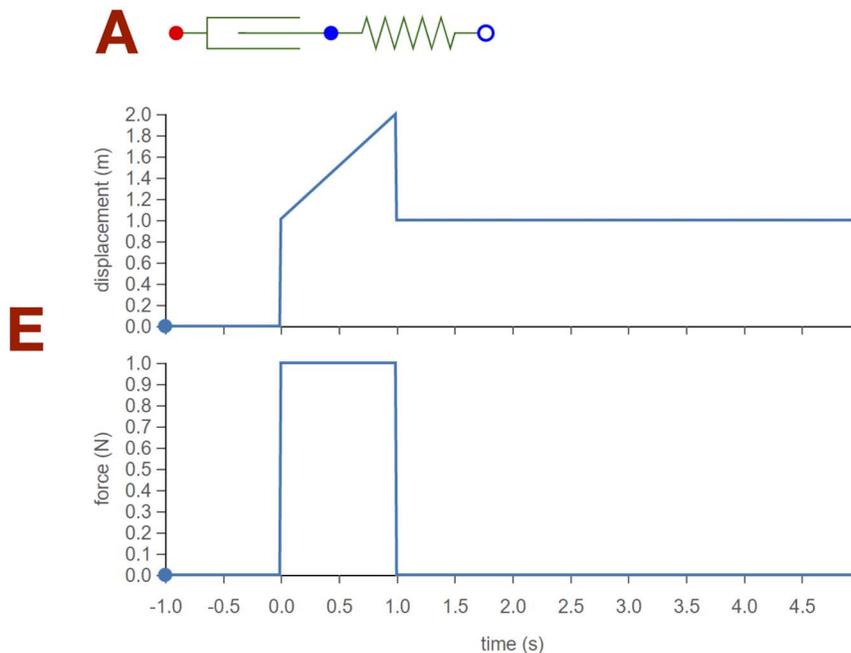


Element properties



System: Maxwell Body

- fixed point
- free point
- plotted fixed point
- plotted free point



G simulation time range

start: s end: s delta t: s

Fig 2. ELViS open mode. In the open mode of ELViS, users can create viscoelastic systems consisting of springs, dashpots, and force generators in a drag and drop editor and simulate the mechanical response to external forces or imposed deformations. The red letters serve as references for the main text.

input and changing the duration and amplitude, the user indirectly varies the speed at which the force or deformation acts on the system. In this way, EIViS allows students to explore the velocity dependence of viscoelastic systems and to understand how dashpots, unlike springs, respond to the velocity of imposed deformations.

The simulation panel (Fig 2E) shows a plot of both the input and calculated response of the system, the latter of which will update instantaneously as one changes system and input parameters. By clicking on the play button (Fig 2F), the user can start a visual dynamic simulation of the mechanical response of the system, which affects both the system's sketch in the drag and drop editor and the plots in the simulation panel. Finally, in the simulation time range menu (Fig 2G), the user can change the simulation start and endpoint, as well as the time intervals of the numeric calculation.

On the basis of the EIViS framework and its possibilities for creating and simulating viscoelastic systems, we also created an interactive online lesson consisting of 13 levels, teaching the basics of viscoelastic modeling. The lesson includes design elements adapted from computer games to increase the students' motivation during the work process, a concept called gamification (32). The gamification design principles used here are levels, progress bars, immediate feedback, and the possibility of multiple attempts to solve a level. The lesson takes about 20 min in total. The first 10 levels teach students the main building blocks of viscoelastic modeling described in section II (i.e., how forces, deformations, spring constants, and damping coefficients add up in series and in parallel. The last 3 levels introduce the Maxwell body, the Voigt body, and the Hill 3-element muscle model.

As an example, Figure 3 shows the user interface of the first level that teaches Hooke's law. In the task windows (Fig 3A), students are given a short explanatory text about the level's problem. The heart of each level is the virtual lab (Fig 3B), where students are presented with a viscoelastic system (a single spring), as well as the appropriate plots for an input (displace-

ment in blue) and output (force in red) signal. Typically, the task of a level is to find the equation that relates the input to the output of the viscoelastic system by varying and combining the system's parameters (the spring constant k) and the input amplitude (the total displacement d) with mathematical operators (+, −, *, /, ⇒), and observing the output until it matches the correct response (Hooke's law).

Alternatively, the task in some of the levels is to construct a viscoelastic model that explains a given input–output relationship by using the drag and drop editor. If the user input in the form of an equation or a viscoelastic model is correct, the level is completed, a short summary window (Fig 3D) recapitulates the learned material, and the student proceeds to the next level.

B. Survey design

We asked students of an undergraduate course in biophysics to take the EIViS lesson, and subsequently, we evaluated their experience with an online survey. All students voluntarily participated in the lesson and subsequent survey. Before the start of the survey, all students gave their written consent to the publication of anonymized survey results. The wording of the consent form can be found in Supplemental Material S2. The survey was designed following principles for an effective evaluation of e-learning methods (33–35). We avoided negative questions or statements (such as “EIViS is not difficult to use”). First, students answered several background questions about previous exposure to viscoelastic modeling. In addition, we asked whether students had watched the lecture videos on viscoelastic modeling (which was part of the biophysics course), whether they participated in the corresponding online exercises, and whether they continued to study the topic on their own, beyond the scope of the course. The students then rated different statements in 4 categories on a scale from 1 (strongly disagree) to 5 (strongly agree). The question categories were the following: technical quality of EIViS, educational quality of EIViS, content and information quality, and user satisfaction. At

ELViS — Lesson

Learning the concepts of **elastic-viscous** systems.

○○○○○○○○○○○○○○○○

A

Single Spring

Question, 1

The first element we need to build viscoelastic systems is the **spring**, the elastic element.

In the **virtual lab**, you can experiment with a spring. Change the **spring constant** k and stretch the spring by a length **displacements** d .

Observe the output **force** F and derive an equation connecting F , k and d .

What force F is generated by a spring with **spring constant** k when it is **stretched** by a length d ?

C

 $F =$

Use the spring constant k , the displacement d , numbers, and the operators $+$, $-$, $*$, $/$, $($, $)$, $=$.

EVALUATE >>

B

Virtual Lab

$k =$ $d =$

input

time (s)

output

time (s)

▶ ◀▶▶

D

Great, you have learned that the force increases **proportionally** with elongation. The factor of proportionality is the spring constant k .

$$F = k \cdot d$$

This relationship is called **Hooke's law**.

CONTINUE >>

Fig 3. ELViS lesson mode. In the ELViS lesson mode, users learn the basic rules of viscoelastic systems and the model systems Maxwell body, Voigt body, and Hill muscle model in 13 game-based levels. The red letters serve as references for the main text.

the end of the survey, the students were given the opportunity to express comments, suggestions, and criticism in a text input field.

The survey was conducted anonymously via a Google Forms document (Google LLC, Mountain View, CA). The link to the survey was only given to students who had successfully completed all levels of the ELViS lesson mode. All survey participants agreed to a privacy statement in which we informed them that the data will be collected anonymously, only be used for teaching and scientific purposes, and that the survey results might be statistically evaluated and presented in aggregated form in scientific publications.

C. Survey results

The results of the background questions are presented in Table 1. Although the biophysics course is offered for both bachelor's and master's students, the survey showed that the majority of the survey participants were master's students in the fields of medical engineering, physics, integrated life sciences (an interdisciplinary natural science course), and life science engineering (biotechnology with an additional engineering focus). All students had previously taken a 2-semester introductory course in experimental physics. The vast majority of survey participants stated that they had regularly attended the biophysics online

Table 1. Background questions answered by 50 students.

Background questions (<i>N</i> = 50)	Answer (<i>N</i>)
What course of study are you enrolled in?	Medical engineering (27) Integrated life sciences (12) Life science engineering (9) Physics (2)
What degree are you aiming for in your current study program?	MSc (39) BSc (11)
Before using EIViS, did you watch the lecture videos on the topic of viscoelastic models, springs, and dashpots?	Yes (45) No (5)
Before using EIViS, did you complete the exercises on viscoelastic modeling accompanying the lecture?	Yes (49) No (1)
Did you conduct your own independent research on the topic of viscoelasticity, in addition to lectures and exercises?	Yes (17) No (33)

lectures and exercises and had, therefore, been exposed to the contents of the EIViS lecture.

The results of the student evaluation of the EIViS lesson are illustrated in Table 2 as mean and standard deviation (SD). The technical quality of EIViS was evaluated as consistently positive by the students. All statements in this category, such as “EIViS is easy to use,” “EIViS is interactive,” and “The EIViS lesson is well

structured,” were rated, on average, with a score of more than 4. The most controversial statement in this section was “EIViS had a nice design,” which the students rated at 4.04 ± 0.99 (mean \pm SD).

The section evaluating the educational quality of EIViS started with perhaps the single most important question of the survey: “Working with EIViS has increased my understanding of

Table 2. Results from a survey of 50 students evaluating EIViS.

EIViS evaluation (<i>N</i> = 50)	Mean \pm SD
Technical quality of EIViS	
EIViS is easy to use.	4.18 ± 0.7
EIViS is user friendly.	4.18 ± 0.78
EIViS is interactive.	4.64 ± 0.64
EIViS runs fast in my browser.	4.84 ± 0.38
The EIViS user interface is well designed.	4.04 ± 0.99
EIViS runs flawlessly in my browser. ^a	4.66 ± 0.63
The EIViS lesson is well structured.	4.54 ± 0.68
Educational quality of EIViS	
Working with EIViS has increased my understanding of viscoelastic systems.	4.2 ± 0.91
EIViS is compatible with my personal learning style.	4.12 ± 0.99
I learned faster with EIViS than I would have with traditional resources (e.g., presentation slides, textbooks).	3.94 ± 1.06
EIViS is a helpful addition to the lecture.	4.36 ± 0.75
The interactive EIViS lecture can completely replace the classical lecture on viscoelastic systems.	2.66 ± 1.28
Content and information quality	
Operating EIViS is intuitive without further instructions. ^a	3.8 ± 0.95
I need additional background knowledge on viscoelastic systems to solve the exercises in the EIViS lessons.	2.72 ± 0.93
The exercises in the EIViS lessons are difficult.	2.04 ± 0.73
The level of difficulty of the exercises in the EIViS lessons is appropriate.	3.96 ± 0.94
The time required to finish all EIViS lessons is acceptable. ^a	4.3 ± 0.77
User satisfaction	
EIViS is fun to use.	4.36 ± 0.56
I am satisfied with the technical performance of EIViS.	4.42 ± 0.65
I am satisfied with the educational quality of EIViS.	4.18 ± 0.78
Overall, I am satisfied with EIViS.	4.28 ± 0.61

^a Further explanations are given in the text.

viscoelastic systems.” The students evaluated this statement with a score of 4.20 ± 0.91 , which demonstrates the didactic success of the EIViS lesson. Interestingly, the majority of students agree with the statement that EIViS is a helpful addition to the existing classical course on biomechanics (mean: 4.36), and some students could even imagine that this interactive e-learning approach could completely replace the corresponding lecture (mean: 2.66). The students rated the level of difficulty of the EIViS lesson as rather easy but appropriate. In an additional question with a free input field (not shown in Table 2), the majority of students stated that they needed between 20 and 30 min (60 min maximum) to complete the EIViS lesson. The majority of students evaluated this time as acceptable (mean: 4.30).

The statement “Operating EIViS is intuitive without further instructions.” was evaluated with 3.80 ± 0.95 . From the open comment section at the end of the evaluation, it became evident that some students had problems understanding how to use the drag and drop editors for creating viscoelastic systems. Two students reported that EIViS was not properly displayed in the browser (one student used Microsoft Edge, and the other student used a tablet). We could not reproduce the technical errors, but after the survey was completed, we implemented into the EIViS lesson an animated image that explains using the drag and drop editor.

The more general statements in the last survey section about user satisfaction confirm that overall, the students thought that the EIViS lesson was fun to use and valuable for educational success. On the basis of the student comments, we have fixed some minor bugs and implemented the following features in the current version of the EIViS lesson in addition to the improvements already mentioned: a progress bar that indicates how much of the lesson the user has already finished, the possibility to move backward to levels that the user already finished, and the possibility to skip a level, if the user repeatedly gives a wrong answer.

IV. CONCLUSION

We developed a JavaScript framework (EIViS) for designing and simulating the mechanical behavior of viscoelastic systems consisting of springs, dashpots, and force generators. On the basis of this framework, we developed an interactive e-learning lesson that teaches the basics of viscoelastic modeling in biophysics. We evaluated the lesson in a survey of 50 students who had previously attended a lecture on biomechanics. The majority of students evaluated the technical and educational quality of the lesson as positive and stated that it increased understanding on the topic. The survey shows that students appreciated the interactive e-learning lesson as a valuable addition to a classical lecture on viscoelastic systems but not as a replacement.

SUPPLEMENTAL MATERIAL

Supplemental material for the mathematical framework and student consent form is available at: <https://doi.org/10.35459/tbp.2020.000169.s1>, and the video at <https://doi.org/10.35459/tbp.2020.000169.s2>.

AUTHOR CONTRIBUTIONS

DK was responsible for conceptualization, methodology, investigation, writing the original draft, with subsequent review and editing, and visualization. BF managed conceptualization, methodology, review and editing of the manuscript, and supervision. RCG handled conceptualization, software, methodology, review and editing of the manuscript, and supervision.

ACKNOWLEDGMENTS

This work was supported by Deutsche Forschungsgemeinschaft (German Research Foundation; project 383071714; grant FA-336/12.1). We thank Mar C ndor for help with the mathematical framework and Verena Hei wolf for help with the student survey design.

REFERENCES

1. Lim, C. T., E. H. Zhou, and S. T. Quek. 2006. Mechanical models for living cells—a review. *J Biomech* 39(2):195–216.
2. Fung, Y. C. 1981. *Biomechanics: Mechanical Properties of Living Tissues*. Springer-Verlag, New York.
3. Hill, A. V. 1949. The abrupt transition from rest to activity in muscle. *Proc R Soc Lond B Biol Sci* 136(884):399–420.
4. Bassett, D. R., Jr. 2002. Scientific contributions of A. V. Hill: exercise physiology pioneer. *J Appl Physiol* 93(5):1567–1582.
5. Hill, A. V. 1997. The heat of shortening and the dynamic constants of muscle. *Proc R Soc Lond B Biol Sci* 126(843):136–195.
6. Hill, A. V. 1922. The maximum work and mechanical efficiency of human muscles, and their most economical speed. *J Physiol* 56(1–2):19–41.

7. Gasser, H. S., and A. V. Hill. 1997. The dynamics of muscular contraction. *Proc R Soc Lond B Biol Sci* 96(678):398–437.
8. Schwarz, U. S., T. Erdmann, and I. B. Bischofs. 2006. Focal adhesions as mechanosensors: the two-spring model. *Biosystems* 83(2):225–232.
9. Jamali, Y., M. Azimi, and M. R. Mofrad. 2010. A sub-cellular viscoelastic model for cell population mechanics. *PLOS ONE* 5(8):e12097.
10. Block, J., H. Witt, A. Candelli, E. J. G. Peterman, G. J. L. Wuite, A. Janshoff, and S. Köster. 2017. Nonlinear loading-rate-dependent force response of individual vimentin intermediate filaments to applied strain. *Phys Rev Lett* 118(4):048101.
11. Funk, J. R., G. W. Hall, J. R. Crandall, and W. D. Pilkey. 2000. Linear and quasi-linear viscoelastic characterization of ankle ligaments. *J Biomech Eng* 122(1):15–22.
12. Bates, J. H. T. 2007. A recruitment model of quasi-linear power-law stress adaptation in lung tissue. *Ann Biomed Eng* 35(7):1165–1174.
13. Huxley, A. F. 1957. Muscle structure and theories of contraction. *Prog Biophys Biophys Chem* 7:255–318.
14. McMahon, T. A. 1984. *Muscles, Reflexes, and Locomotion*. Princeton University Press, NJ.
15. Fredberg, J. J., K. A. Jones, M. Nathan, S. Raboudi, Y. S. Prakash, S. A. Shore, J. P. Butler, and G. C. Sieck. 1996. Friction in airway smooth muscle: mechanism, latch, and implications in asthma. *J Appl Physiol* 81(6):2703–2712.
16. Lieleg, O., K. M. Schmoller, M. M. Claessens, and A. R. Bausch. 2009. Cytoskeletal polymer networks: viscoelastic properties are determined by the microscopic interaction potential of cross-links. *Biophys J* 96(11):4725–4732.
17. Gardel, M. L., J. H. Shin, F. C. MacKintosh, L. Mahadevan, P. Matsudaira, and D. A. Weitz. 2004. Elastic behavior of cross-linked and bundled actin networks. *Science* 304(5675):1301–1305.
18. Gittes, F., and F. C. MacKintosh. 1998. Dynamic shear modulus of a semiflexible polymer network. *Phys Rev E* 58(2):R1241–R1244.
19. Kohlrusch, F. 1866. Beiträge zur Kenntniss der elastischen Nachwirkung. *Ann Phys* 204(5):1–20.
20. Thurston, G. B. 1972. Viscoelasticity of human blood. *Biophys J* 12(9):1205–1217.
21. Stone, H. O., H. K. Thompson, Jr., and K. Schmidt-Nielsen. 1968. Influence of erythrocytes on blood viscosity. *Am J Physiol* 214(4):913–918.
22. Miller, L. H., S. Usami, and S. Chien. 1971. Alteration in the rheologic properties of *Plasmodium knowlesi*-infected red cells. A possible mechanism for capillary obstruction. *J Clin Invest* 50(7):1451–1455.
23. Mahdi, A., N. Meshkat, and S. Sullivant. 2014. Structural identifiability of viscoelastic mechanical systems. *PLOS ONE* 9(2):e86411.
24. Kalita, P., and Schaefer R. 2008. Mechanical models of artery walls. *Arch Comput Method E* 15(1):1–36.
25. Holmes, J. W. 2006. Teaching from classic papers: Hill's model of muscle contraction. *Adv Physiol Educ* 30(2):67–72.
26. Leineweber, M. 2020. Take-home tensile testing system for biomechanics education. *Biophysicist* 1(2):6.
27. Howard, J. 2001. *Mechanics of Motor Proteins and the Cytoskeleton*. Sinauer Associates, Sunderland, MA.
28. Jacobs, C. R., H. Huang, and R. Y. Kwon. 2013. *Introduction to Cell Mechanics and Mechanobiology*. Garland Science, New York.
29. Thomson, W. T. 1960. *Laplace Transformation*. 2nd edition. Prentice-Hall, Englewood Cliffs, NJ.
30. D'Azzo, J. J., C. H. Houpis, and S. N. Sheldon. 2003. *Linear Control System Analysis and Design with MATLAB*. 5th edition. Marcel Dekker, New York.
31. Bostock, M., V. Ogievetsky, and J. Heer. 2011. D³: Data-driven documents. *IEEE Trans Vis Comput Graph* 17(12):2301–2309.
32. Dicheva, D., C. Dichev, G. Agre, and G. Angelova. 2015. Gamification in education: a systematic mapping study. *Educ Technol Soc* 18(3):75–88.
33. Mandinach, E. B. 2005. The development of effective evaluation methods for e-learning: a concept paper and action plan. *Teach Coll Rec* 107(8):1814–1835.
34. Hassanzadeh, A., F. Kanaani, and S. Elahi. 2012. A model for measuring e-learning systems success in universities. *Expert Syst Appl* 39(12):10959–10966.
35. Motiwalla, L. F. 2007. Mobile learning: a framework and evaluation. *Comput Educ* 49(3):581–596.